



Cite as

Nano-Micro Lett.
(2024) 16:274

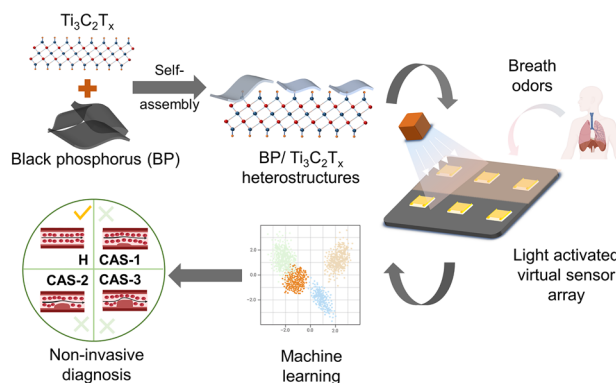
Light-Activated Virtual Sensor Array with Machine Learning for Non-Invasive Diagnosis of Coronary Heart Disease

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Accepted: 6 July 2024
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HIGHLIGHTS

- Photoresponsive black phosphorus (BP)/Ti₃C₂T_x composites were synthesized by a self-assembly strategy.
- Enhanced gas sensitive property was achieved by visible light modulation.
- Light activated virtual sensor array was fabricated based on BP/Ti₃C₂T_x composite.
- Diagnosis of coronary heart disease was achieved with the help of machine learning.

ABSTRACT Early non-invasive diagnosis of coronary heart disease (CHD) is critical. However, it is challenging to achieve accurate CHD diagnosis via detecting breath. In this work, heterostructured complexes of black phosphorus (BP) and two-dimensional carbide and nitride (MXene) with high gas sensitivity and photo responsiveness were formulated using a self-assembly strategy. A light-activated virtual sensor array (LAVSA) based on BP/Ti₃C₂T_x was prepared under photo-modulation and further assembled into an instant gas sensing platform (IGSP). In addition, a machine learning (ML) algorithm was introduced to help the IGSP detect and recognize the signals of breath samples to diagnose CHD. Due to the synergistic effect of BP and Ti₃C₂T_x as



well as photo excitation, the synthesized heterostructured complexes exhibited higher performance than pristine Ti₃C₂T_x, with a response value 26% higher than that of pristine Ti₃C₂T_x. In addition, with the help of a pattern recognition algorithm, LAVSA successfully detected and identified 15 odor molecules affiliated with alcohols, ketones, aldehydes, esters, and acids. Meanwhile, with the assistance of ML, the IGSP achieved 69.2% accuracy in detecting the breath odor of 45 volunteers from healthy people and CHD patients. In conclusion, an immediate, low-cost, and accurate prototype was designed and fabricated for the noninvasive diagnosis of CHD, which provided a generalized solution for diagnosing other diseases and other more complex application scenarios.

KEYWORDS Black phosphorus/MXene heterostructures; Light-activated virtual sensor array; Diagnosis of coronary heart disease; Machine learning

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Published online: 16 August 2024



SHANGHAI JIAO TONG UNIVERSITY PRESS

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1 Introduction

Coronary heart disease (CHD) is one of the most important causes of death worldwide, causing millions of direct deaths each year and numerous sequelae such as disability, cardiac enlargement, and cardiac arrhythmias, so early diagnosis and prevention of CHD is of great significance [1–3]. Diagnostic modalities for CHD such as cardiac stress test, ambulatory electrocardiogram, and coronary computed tomography (CT) angiography, although playing an essential role in the clinic, often require the use of major instruments or complex operations, which hinders the timely detection and treatment of CHD. Therefore, there is an urgent need for a simple, rapid, and accurate testing modality [4–6]. Some studies have reported that human breath has the potential to serve as a new diagnostic source because it contains specific disease markers. For example, the correlation between the concentration of respiratory ammonia and blood urea was explored, and some researchers studied the correlation between exhaled isoprene and blood cholesterol [7, 8]. Regarding CHD, ischemic-damaged cardiomyocytes produce unique biomarkers that will be released through respiration [9]. This demonstrates that exhaled gas is a highly promising candidate for performing noninvasive diagnosis of CHD.

Current gas sensing technologies often rely on large specialized equipment such as tunable diode laser absorption spectroscopy (TDLAS), non-dispersive infrared (NDIR) gas sensors, and ultraviolet-differential optical absorption spectroscopy (UV-DOAS) [10–12]. These technologies with great achievements are widely used in various fields and have an irreplaceable position. However, these devices are not only costly, but also complicated sampling and pre-processing processes make the system response slow, lack portability and ease of operation, and make it difficult to meet the demand for real-time response. Therefore, developing a portable, easy-to-operate, and accurate instant gas sensing platform (IGSP) is significant for the non-invasive diagnosis of CHD patients. The IGSP consists of three parts: the gas sensing module, the signal transmission module, and the data storage and processing module [13]. Among them, the gas sensing module is the most essential part, as its ability to distinguish between different gases determines the accuracy of IGSP. Therefore, it is of great significance to develop an accurate gas sensing module and further build the IGSP based on it.

The design aspects of high-performance gas sensing modules have been extensively studied, and researchers have gained inspiration from nature (Fig. 1a). Humans and other mammals can recognize the distinctive odors of volatile chemicals, an ability that stems from the presence of hundreds of subtypes of receptors [14, 15]. Different combinations of receptors can produce unique signals corresponding to various odors. Inspired by this, the sensor array (SA) has been extensively studied [16, 17]. SA consists of multiple sensors of different compositions that are capable of producing unique signals for various odors. For example, one SA for fire detection was prepared using twelve different sensors and achieved 100% accuracy and 85% sensitivity, and another SA consisting of four metal oxide semiconductors, including SnO₂, In₂O₃, WO₃, and CuO, detected a variety of volatile organic compounds (VOCs) with 98% accuracy [18, 19]. Although the current study is fruitful in the design of SA, the lack of performance of individual sensors and the number of sensors facing diminishing marginal effects need to be addressed.

Sensing materials are the basis for building the SA, with sensitivity and selectivity being key performance indicators. Current commercial chemiresistive gas sensors based on metal oxide semiconductors (MOS: SnO₂, In₂O₃, and CuO et al.) have mature technology and are widely used in industrial processes due to high sensitivity and low cost [20–22]. However, MOS materials face high operating temperatures as well as insufficient selectivity, leading to limitations in their further applications [23, 24]. Other materials such as conductive polymers and perovskites face poor stability and insufficient sensitivity, which are still a long way from practical application [25, 26]. For the performance enhancement of sensing materials, some researchers have explored the potential of novel materials for gas sensing. MXene, a novel two-dimensional (2D) material, is considered to have great potential in gas sensing due to its unique layered structure, excellent electrical conductivity, and abundant terminal groups [27]. For example, a Ti₃C₂T_x MXene based gas sensors owned good gas-sensing performance with detection limits as low as 50 ppb for VOCs [28]. However, the pristine MXene is similar to other 2D materials and suffers from insufficient selectivity and stability. The good thing is that the gas-sensitive performance has much room for improvement due to its abundant terminal groups [29, 30].

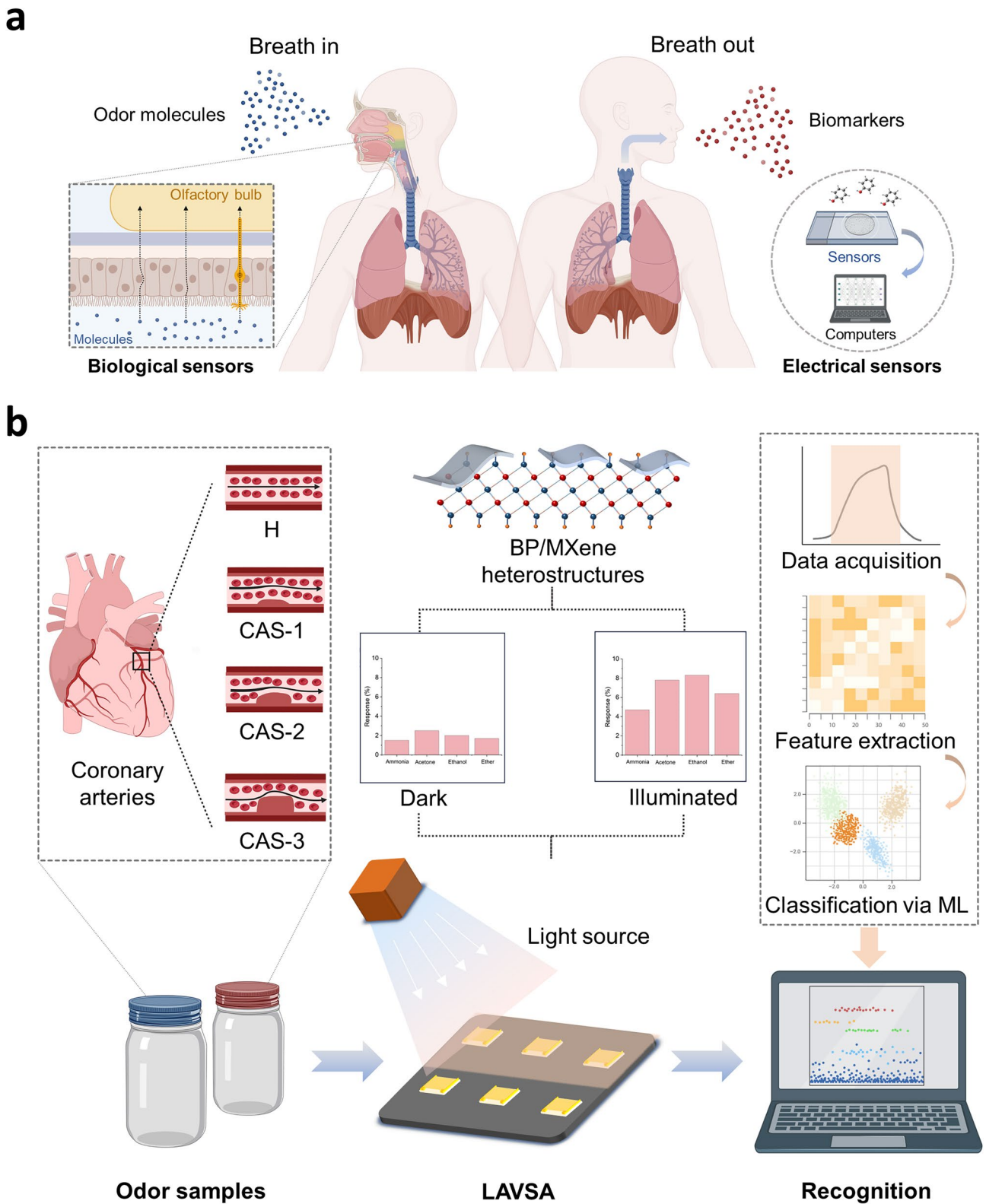


Fig. 1 Disease recognition by breath odor through IGSP. **a** Light-activated gas sensing design that mimics the natural olfactory system. **b** Gas detection through IGSP and recognition of different diseases using ML. Figures were created with BioRender

To enhance the gas-sensing performance of MXene-based sensors, chemical modification of MXene nanosheets with second-phase materials is a widely investigated approach. The sensing performance of pristine MXene was improved by changing its structural and electrical properties. In addition, due to the increase in the specific surface area of the composite material, it leads to an increase in the number of active sites for adsorbed gas molecules, which enables better sensitivity to be obtained [31, 32]. For example, in-situ growth of MAPbBr₃ perovskite on the surface of Ti₃C₂T_x resulted in a 37%–70% increase in response, and the response speed of W₁₈O₄₉/Ti₃C₂T_x composite material was enhanced to 5.6 s [33, 34]. After chemical modification, the stability, sensitivity, and response time were improved to different degrees, which proved that the strategy was effective. However, the choice of the second phase determines the upper limit of the performance enhancement of the composites formed with MXene.

Conventional studies have mainly focused on material replacement or chemical modification, but the degree of improvement usually depends on the gas-sensitive properties of the modifier, which imposes limitations on practical use. In fact, physical environment modification, such as light modulation, is a novel idea of modulation. Changes in the physical environment, such as light, can have an effect on the physicochemical properties of the material, such as faster electron transfer and faster adsorption–desorption processes [35–37]. For example, the response of MoS₂–NO₂ was enhanced by 25% using visible light modulation [38]. Inspired by the photosensitizing effect of MXene materials in the range of near-infrared light to visible light, external physical modulation can be utilized to improve the performance of gas sensors based on MXene materials [39, 40]. The introduction of light illumination may result in intrinsic absorption of photons and accelerate the electron transfer between the material surface and the gas molecules. In addition, as other photosensitive materials including MOS and black phosphorus (BP) can form complexes with MXene, not only the light can promote the electron transfer, but also the synergistic effect between the two substances can promote the gas sensing performance [41]. BP is a 2D photosensitive material, and the absorbed light range overlaps with that of MXene as well as be able to form a heterostructure with MXene. Therefore, BP can be a strong competitor for MXene modifiers and has a synergistic effect with MXene when light is introduced [42, 43]. However, there are

few reports on BP/MXene complexes as gas sensing feedstock under light modulation. In addition to the material design, the construction strategy of the SA is also important. In principle, the greater the number of sensors, the more accurate the characterization of the gas. However, it also faces diminishing marginal benefits. Inspired by the light modulation strategy, the light-activated virtual sensor array (LAVSA) is proposed, where the SA is tested for gases with and without light conditions separately. It is equivalent to doubling the number of sensors in the SA, enabling a more accurate portrayal of the target gas. This strategy can geometrically increase the efficiency of SA. However, there are few reports on LAVSA in the field of gas sensing, let alone the IGSP based on it.

In addition to the study of materials, the algorithms used to process the data have a significant impact on the performance of the IGSP. Because of the large amount of data obtained from experiments, accurately extracting features from different samples and classifying them is the crux of the problem. Machine learning (ML) algorithms, a category of Artificial Intelligence, are able to simulate humans to learn and analyze data by monitoring and distinguishing relationships between data. There are many algorithms of ML based on different principles, such as Support Vector Machines (SVMs) and Naive Bayes (NB) [44]. Due to its ability to extract features from large amounts of data, ML has many applications in diagnosing and predicting different diseases. For example, Gupta et al. used NB algorithm to estimate the risk of coronary heart disease with an accuracy of 0.93 [45]. In addition, Joloudari et al. used Decision Tree (DT) algorithm for coronary heart disease diagnosis with an accuracy of 91.47% [46]. However, there are few studies on using ML for gas sensing systems, let alone diagnosing coronary heart disease via gas samples.

Based on the above research ideas and current status, this work aims to prepare LAVSA with high gas-sensing properties by MXene-based photoresponsive composites and further fabricate easy-to-operate and accurate IGSP (Fig. 1b). Further, the prepared IGSP was used for the detection and noninvasive diagnosis of exhaled breath of CHD patients and healthy individuals with the help of the ML algorithm. BP/Ti₃C₂T_x complexes were first synthesized by self-assembly strategy and prepared as sensors. As a proof-of-concept, detection was performed using typical gases, including ammonia, acetone, ethanol, and ether, to explore the optimal composition, light wavelengths and

intensities, and the enhancement of sensing performance of BP/Ti₃C₂T_x. Subsequently, a six-dimensional LAVSA was fabricated based on three materials, i.e., pure Ti₃C₂T_x, pure BP, and BP/Ti₃C₂T_x composite. Fifteen odor molecules, which are widely present in nature, were tested with and without illumination to examine the gas recognition performance of LAVSA. Based on this, an IGSP was prepared using the LAVSA and Arduino platform, which was applied for the non-invasive diagnosis of CHD patients. A total of 45 breath samples from CHD patients and healthy individuals were examined using IGSP for identification and diagnosis with the help of ML. In a word, this work developed a LAVSA-based IGSP, which provided a new strategy for the construction of the SA and noninvasive diagnosis of CHD, and provides ideas for noninvasive and immediate detection of other diseases such as cancer and gastric diseases.

2 Experimental Section

2.1 Materials

Lithium fluoride (LiF, 99.99%, 100 μm) was supplied by Merck Co., Ltd. Ti₃AlC₂ powder (90%, 40 μm) was supplied by Merck Co., Ltd. Hydrochloric acid (HCl, AR) was supplied by Meryer Co., Ltd. N, N-dimethylformamide (DMF, SafeDry) was supplied by Aladdin Co., Ltd. Tetrabutylammonium hydroxide (TBAOH, 40%) was supplied by Bidepharm Co., Ltd. Black phosphorous (AR, 99.9%) nanosheets were purchased from Zhongke Materials Co., Ltd.

2.2 Preparation of Few-Layer Ti₃C₂T_x Nanosheets

Ti₃C₂T_x nanosheets dispersed in DMF were prepared using the tuned microenvironment method. In a polytetrafluoroethylene (PTFE) reactor, 4 g of LiF was added to 80 mL of 9 M HCl solution and stirred at 35 °C for 60 min to dissolve. Then, 4 g of Ti₃AlC₂ was added and stirred at 35 °C and 1000 rpm for 24 h. Finally, the collected multilayer Ti₃C₂T_x MXene is freeze-dried for 36 h. Then, 1 g of multilayer Ti₃C₂T_x powder was added to 24 mL of 25% TBAOH solution. The resulting product was stirred at 500 rpm for 6 h at room temperature for intercalation. Excess TBAOH was then washed off with ethanol, and all precipitate was collected in

a 100 mL centrifuge tube. Approximately 60 mL of DMF was then added to the centrifuge tube and shaken until the precipitate completely disappeared. The upper liquid layer was collected by centrifugation at 12,000 rpm for 5 min. DMF was added and centrifuged repeatedly until a 50 mL solution was collected with a concentration of approximately 5 mg mL⁻¹ of MXene.

2.3 Preparation of BP/Ti₃C₂T_x Composite

To prepare BP/Ti₃C₂T_x composite, 20 mL of MXene DMF (~5 mg mL⁻¹) solution was added to the reactor, and then 0.1 g of BP nanosheets was added for the self-assembly process. The mixture was shaken for 30 s to obtain a targeted homogeneous black solution. A portion of the solution was dried to obtain solids, and the composite was denoted as BP/Ti₃C₂T_x.

2.4 Preparation of Light-Activated Virtual Sensor Array (LAVSA)

0.5 mL solutions of the Ti₃C₂T_x, BP, and BP/Ti₃C₂T_x were added to 10 mL of DMF, respectively, to obtain three solutions as the primary sources for the gas-sensitive films. Then, three interdigital electrodes served as the backbone of LAVSA. A spray gun was utilized to evenly apply 2 mL of each solution of the three synthesized materials to the interdigital electrode, and then electrodes were dried in a vacuum oven at 60 °C for 2 h to form a gas-sensitive film. The LAVSA was used in the presence and absence of light to obtain six-dimensional data. Each sensor of the obtained MBA was recorded as Sensor 1: (without light) BP/Ti₃C₂T_x, Sensor 2: (under light) BP/Ti₃C₂T_x, Sensor 3: (without light) Ti₃C₂T_x, Sensor 4: (under light) Ti₃C₂T_x, Sensor 5: (without light) BP, and Sensor 6: (under light) BP.

2.5 Structural Characterizations

X-ray diffraction (XRD, MiniFlex600, Rigaku, Japan) was performed using Cu Kα radiation (λ=0.15406 nm) at a voltage of 40 kV, a current of 15 mA, a scanning frequency of 0.083° s⁻¹, and a scanning range of 3°–60° in the 2θ region to explore crystal properties. The surface morphology was characterized using a field emission scanning electron

microscope (FESEM: SU8220, HITACHI, Japan) equipped with an energy-dispersive X-ray spectrometer (EDS) with an accelerating voltage of 10 kV. The shape and morphology were analyzed with a high-resolution transmission electron microscope (HRTEM: JEM2010, JEOL, Japan) to observe the lattice of $\text{Ti}_3\text{C}_2\text{T}_x$. X-ray photoelectron spectroscopy (XPS) analysis was performed on an X-ray photoelectron spectrometer (AXIS Supra+, Kratos, UK) using an Al K α X-ray source to investigate the surface electronic states. The morphology and thickness of the samples on silicon substrates were studied using an atomic force microscope (AFM: Dimension ICON, Bruker, Germany) in ScanASYST mode. Gas chromatography-mass spectrometry (QP2010 ultra, Shimadzu, Japan) was used to identify the components in odor samples from different volunteers.

2.6 Dynamic Gas Sensing Experiment

Gas sensing measurements were made at room temperature using a self-built Instant gas sensing platform (IGSP). A 1.2-L vessel was used as a vapor-sensing chamber. During the experiment, different volumes of the gas solution to be tested were directly fed into the vessel through a hole located on the upper surface of the vessel. After injection, the vessel was sealed with transparent tape. The concentration of the test gas was determined by the following calculation:

$$C(\text{ppm}) = \frac{\rho \cdot V \cdot \omega}{M} \cdot \frac{V_m}{V_c} \times 10^6$$

where ρ (g mL^{-1}) is the density of the gas molecule; V (μL) is the volume of the gas molecule solution; ω (%) is the mass fraction of the gas molecule solution; M (g mol^{-1}) is the molar mass of the gas molecule; V_m (L mol^{-1}) is the molar volume of the ideal gas; V_c (L) is the volume of the vapor sensing chamber.

Resistance values were recorded under steady-state conditions after exposure to pure air and air containing the target gas using an Arduino-based gas sensing system. The Arduino board facilitated data acquisition and storage for dynamic gas detection. An advanced computer program collected data from all sensors at a constant rate. The applied DC voltage had an amplitude of 5 V and a measurement error of less than 0.1%.

2.7 Identification of CHD Patients via Breath Odors

The IGSP was applied to detect and identify respiratory gases in different populations. In all, 45 volunteers took part in this study, including 10 healthy individuals (H), 11 patients with degree of CAS 0–25% (CAS-1), 9 patients with degree of CAS 25%–50% (CAS-2), and 15 patients with degree of CAS more than 50% (CAS-3). Before the study, informed written consent was obtained from all participants. The approval from the institutional ethics committee, Biomedical Research Ethics Committee, Department of Cardiology, Beijing Tsinghua Changgung Hospital was obtained prior to the research (approval number: 24034–4-01).

Before the experiment, well-sealed aluminum gas collecting bags with a volume of 1 L were used to collect the exhaled gas from volunteers. The outlet of the bag then delivered the gas smoothly to the LAVSA over a distance of 2 cm for 10 s. The computer recorded the change in LAVSA resistance in real-time. To ensure the stability of the experiment, 20 s were spaced between each delivery to restore the baseline resistance of the LAVSA. A total of 20 consecutive experiments in the presence and absence were performed on breath samples from each volunteer.

3 Results and Discussion

3.1 Fabrication and Characterization of BP/ $\text{Ti}_3\text{C}_2\text{T}_x$ -Based Composite and Gas Sensor

The core components of a gas sensor were sensing materials with different properties. MXene nanosheets were prepared using the tuned microenvironment method (Fig. S1) [47]. Due to the ease of tunability of MXene surface groups, forming composites with different materials was a means to significantly improve gas sensing performance. As shown in Fig. S2, BP/ $\text{Ti}_3\text{C}_2\text{T}_x$ composites were prepared by a self-assembly process, and their surface morphology, physical and chemical structures were characterized. The $\text{Ti}_3\text{C}_2\text{T}_x$, BP, and BP/ $\text{Ti}_3\text{C}_2\text{T}_x$ solutions were shown in Fig. S3. As shown in Fig. 2a, the gas sensor consisted of a substrate, an electrode, and a gas-sensitive membrane. The specific preparation process was to fix an interdigital electrode on the polyethylene terephthalate (PET) substrate as the backbone of the gas sensor, and then the synthesized composite was uniformly sprayed on the interdigital electrode to form

a gas-sensitive membrane. The fabricated gas sensor was shown in Fig. 2b.

To study the surface morphology of the material, the samples were observed using scanning electron microscopy (SEM), transmission electron microscopy (TEM), and atomic force microscopy (AFM). The morphology of $\text{Ti}_3\text{C}_2\text{T}_x$ nanosheets was shown in TEM images (Fig. 2c) as uniform thin layers, indicating a typical two-dimensional structure. The thickness of $\text{Ti}_3\text{C}_2\text{T}_x$ nanosheets was shown to be around 3 nm in the AFM images (Fig. S5a, b), which was consistent with the TEM results [48]. The images of TEM of BP also showed a stacked sheet structure (Fig. 2d), indicating the two-dimensional material properties of BP. The thickness of BP nanosheets was shown to be around 30 nm in the AFM images and was uniform in thickness (Fig. S5c, d) [49]. The TEM images of the heterostructures of BP/ $\text{Ti}_3\text{C}_2\text{T}_x$ showed the self-assembly of BP nanosheets on the surface of $\text{Ti}_3\text{C}_2\text{T}_x$ nanosheets (Fig. 2e). To further investigate the BP/ $\text{Ti}_3\text{C}_2\text{T}_x$ heterostructure, high-resolution transmission electron microscopy (HRTEM) was employed to observe the crystal properties. The HRTEM images (Fig. 2f) of the BP/ $\text{Ti}_3\text{C}_2\text{T}_x$ heterostructure showed that there were two distinctly different widths of lattice spacings of 0.27 and 0.34 nm, which corresponded to the (002) plane of the $\text{Ti}_3\text{C}_2\text{T}_x$ and the (020) plane of BP [43, 50, 51]. The corresponding selected area electron diffraction (SAED) patterns (Fig. 2g) showed bright spots consistent with the lattice spacing, indicating that the BP/ $\text{Ti}_3\text{C}_2\text{T}_x$ heterostructures exhibit typical crystalline properties. The elemental distribution and film-forming morphology of the samples were examined by SEM and energy dispersive spectroscopy (EDS). SEM images of pure $\text{Ti}_3\text{C}_2\text{T}_x$ (Fig. S4b) showed the formation of a uniform film, indicating the successful preparation of $\text{Ti}_3\text{C}_2\text{T}_x$ nanosheets, and the uniform distribution of Ti, O, and C elements can be seen by EDS elemental mapping. The SEM images of BP showed the successful preparation of BP nanosheets, and the uniform distribution of P could be seen by EDS elemental mapping (Fig. S4a). The SEM images of the composites demonstrated a stacked membrane-like structure, proving that BP self-assembled on $\text{Ti}_3\text{C}_2\text{T}_x$ to form a nanocomposite structure. EDS elemental mapping confirmed the distribution of elements C, O, P, and Ti in the BP/ $\text{Ti}_3\text{C}_2\text{T}_x$ nanocomposites (Fig. 2h, i), suggesting that BP self-assembled on $\text{Ti}_3\text{C}_2\text{T}_x$. In summary, the surface morphology and elemental distribution based on BP, $\text{Ti}_3\text{C}_2\text{T}_x$, and BP/ $\text{Ti}_3\text{C}_2\text{T}_x$ indicated that BP was successfully

self-assembled onto $\text{Ti}_3\text{C}_2\text{T}_x$ and formed a heterogeneous structure.

The synthesized BP/ $\text{Ti}_3\text{C}_2\text{T}_x$ composites, $\text{Ti}_3\text{C}_2\text{T}_x$, and BP were analyzed by XRD to determine the crystal structure and phase composition. The characteristic diffraction peaks of BP were located at $2\theta = 17.5^\circ$ and 34.9° corresponding to (020) and (040) crystal planes, respectively [52, 53]. $\text{Ti}_3\text{C}_2\text{T}_x$ had a distinct cusp at about 7.1° corresponding to the (002) crystal plane [54, 55]. The heterostructure of BP/ $\text{Ti}_3\text{C}_2\text{T}_x$ was mainly confirmed by observing whether the diffraction peaks of BP and $\text{Ti}_3\text{C}_2\text{T}_x$ nanosheets were present at the same time or not. As BP self-assembled onto the surface of $\text{Ti}_3\text{C}_2\text{T}_x$, the peak intensity of $\text{Ti}_3\text{C}_2\text{T}_x$ gradually decreased (Fig. 3a). This was due to the fact that X-rays needed to penetrate the BP nanosheets in order to reach the $\text{Ti}_3\text{C}_2\text{T}_x$ layer underneath, which led to a decrease in the peak intensity of $\text{Ti}_3\text{C}_2\text{T}_x$. The simultaneous appearance of the characteristic peaks of BP and $\text{Ti}_3\text{C}_2\text{T}_x$ in the XRD spectra proved the successful formation of the BP/ $\text{Ti}_3\text{C}_2\text{T}_x$ heterostructures with a good crystal structure.

XPS analysis was performed to investigate the surface chemical composition and bonding state of the BP/ $\text{Ti}_3\text{C}_2\text{T}_x$ composites. The wide spectrum (Fig. 3b) showed the presence of Ti, C, P, O, F, and N elements in the BP/ $\text{Ti}_3\text{C}_2\text{T}_x$ nanocomposites. The high-resolution C 1s spectrum (Fig. 3c) showed three components at 281.21, 284.53, and 286.47 eV, corresponding to C–Ti–O, C–C, and C–O, respectively [56, 57]. The high-resolution O 1s spectrum (Fig. 3d) showed two strong peaks at 529.95 and 532.27 eV, corresponding to C–Ti–O and Ti–O–P, respectively [56–58]. The high-resolution P 2p spectrum (Fig. 3e) observed strong peaks at 129.72 and 130.83 eV corresponding to P 2p_{3/2} and P 2p_{1/2}, respectively, as well as at 134.12 eV corresponding to P_xO_y, confirming BP self-assembled in $\text{Ti}_3\text{C}_2\text{T}_x$ [52, 59]. High-resolution Ti 2p spectrum (Fig. 3f) showed two double peaks with an area ratio of 1:2, i.e., Ti 2p_{1/2} and Ti 2p_{3/2}. Two strong peaks of Ti 2p_{3/2} were observed at 455.32 and 456.51 eV, corresponding to Ti–C and Ti–T_x, respectively [55, 60, 61]. It suggested that in $\text{Ti}_3\text{C}_2\text{T}_x$, Ti–C, and Ti–T_x bonds were the dominant chemical state of Ti, and there was no material oxidation. In conclusion, the XPS analysis revealed important information about the chemical composition and bonding states for the BP/ $\text{Ti}_3\text{C}_2\text{T}_x$ heterostructure, providing evidence for the successful preparation of the complex.

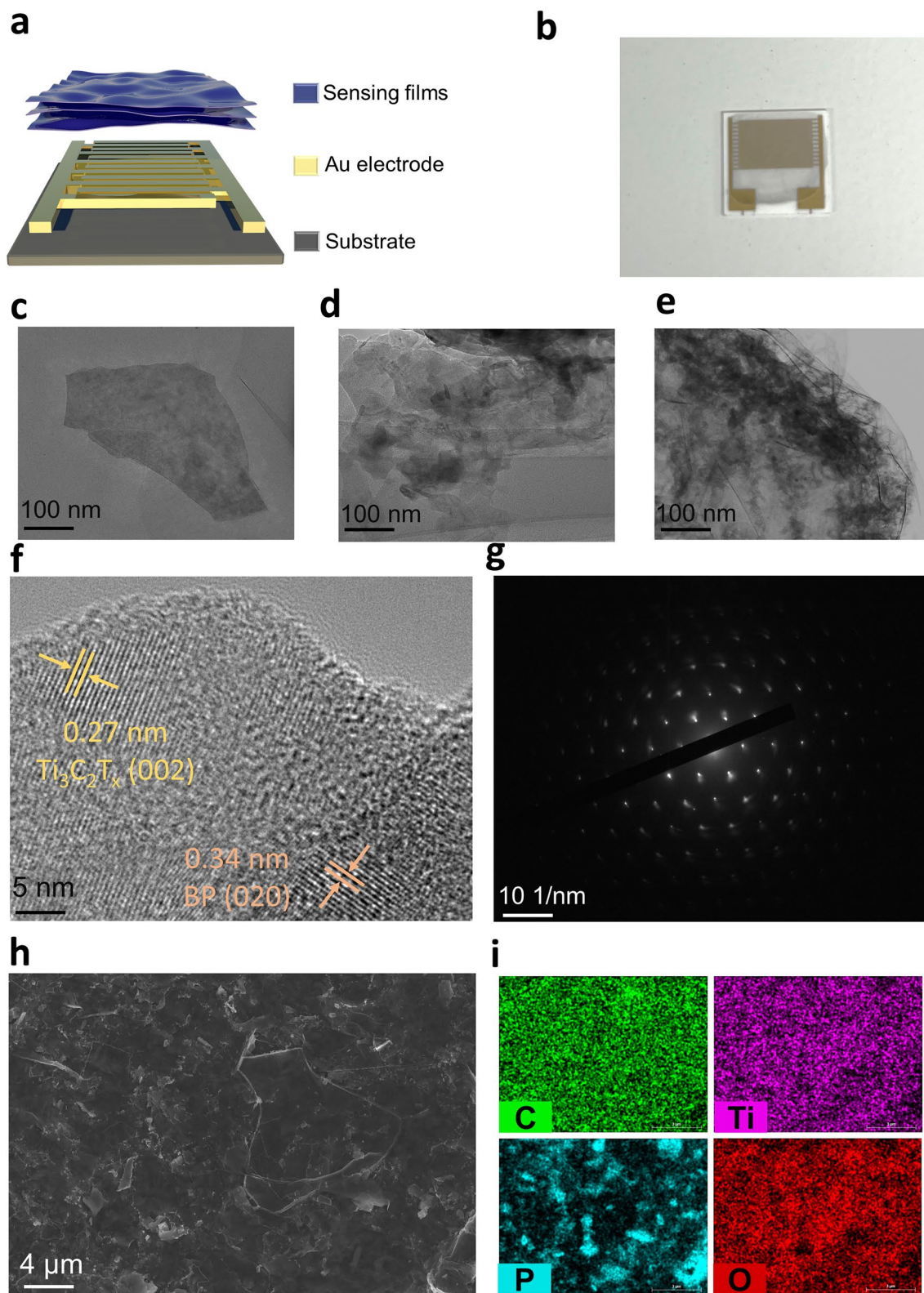


Fig. 2 Physical, micro, and crystal structure of the gas sensor. **a** Diagram of the physical structure of the gas sensor. **b** Real picture of the gas sensor. TEM Images of **c** $\text{Ti}_3\text{C}_2\text{T}_x$ nanosheets, **d** BP nanosheets and **e** $\text{BP}/\text{Ti}_3\text{C}_2\text{T}_x$ composite. **f** Image of HRTEM of $\text{BP}/\text{Ti}_3\text{C}_2\text{T}_x$ composite. **g** Image of SAED pattern of $\text{BP}/\text{Ti}_3\text{C}_2\text{T}_x$ composite. **h** Image of SEM of the surface of $\text{BP}/\text{Ti}_3\text{C}_2\text{T}_x$ composite. **i** Image of EDS elemental mapping of $\text{BP}/\text{Ti}_3\text{C}_2\text{T}_x$ composite

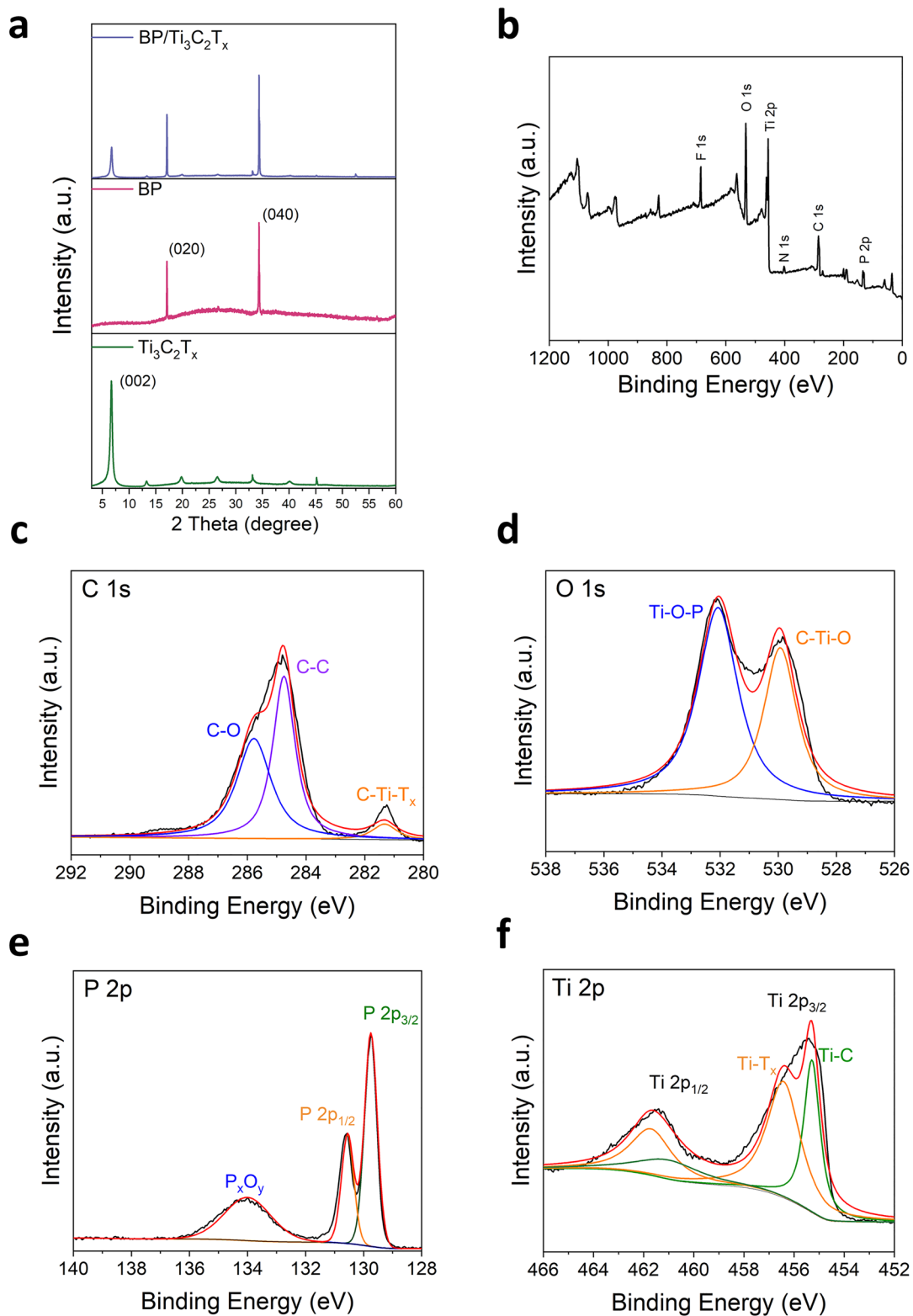


Fig. 3 Characterization of crystal and chemical properties. **a** Image of XRD of BP, Ti₃C₂T_x, and BP/Ti₃C₂T_x composite. **b** XPS survey spectrum of BP/Ti₃C₂T_x composite and high-resolution XPS spectra of **c** C 1s, **d** O 1s, **e** P 2p and **f** Ti 2p in BP/Ti₃C₂T_x composite, respectively

3.2 Sensing Properties of BP/Ti₃C₂T_x Composite

The performance of dynamic response to gas was one of the most important criteria for judging the goodness of a gas sensor. The sensor response was defined as $\frac{R_g - R_a}{R_a} \times 100\%$, where R_a was the initial resistance of the sensor in air, and R_g was the resistance of the sensor when exposed to the target gas. In this work, experiments were designed based on the law of conservation of matter and the principle of gas–liquid equilibrium, and the experimental setup consisted of a sensing module, a data transmission platform, and a data processing module (Fig. 4a). In the experiment, the sensor was placed in a target gas environment with changing concentration in a closed chamber to examine the dynamic response. The gas concentration was varied by dropping different volumes of a solution of gas molecules (Fig. 4b), which utilized the ability of the solution and the gas molecules to form a gas–liquid phase equilibrium [62]. An analog signal was acquired through the sensor, which was then converted into an electrical signal and transmitted to a data processor.

The introduction of light modulation to enhance the gas-sensitive properties of the sensors was a promising way. In this work, BP was self-assembled onto the MXene surface to form BP/Ti₃C₂T_x composite and prepared as gas sensors. As a validation experiment, different ratios of BP/Ti₃C₂T_x sensors were synthesized and tested for typical gases such as acetone, ammonia, ether, and ethanol under different wavelengths and intensities of light modulation to determine the optimal ratios as well as the optimal light conditions.

Firstly, the optimal ratio between BP and Ti₃C₂T_x, as well as the optimal light wavelength and intensity, were explored and tested using acetone. Since the light absorption ranges of A and B were between the visible and near-infrared, representative wavelengths of 420 and 800 nm were selected for the study, according to previous reports [63–66]. It could be seen that the sensor response was different at wavelengths of 420 and 800 nm light (Figs. 4c and S6), and the sensor had a higher response at 420 nm. In addition, as the BP content increased, the sensor response had a convex function nature with the highest response at a mass fraction of 1:1. In addition, with the gradual increase in light intensity, the sensor response also had a convex function nature and had the highest response at a light intensity of 5 mW cm⁻². In summary, the sensor had the optimal response when the illumination

was at 420 nm, the intensity was 5 mW cm⁻² and the mass fraction ratio of BP and Ti₃C₂T_x was 1:1, and the following experiments were based on this condition.

To compare the effect of light on the response, gases from 50 ppb to 5 ppm were tested by the BP/Ti₃C₂T_x-based sensor in the presence and absence of light, respectively. Figure 4d and Fig. S7a–c showed the real-time resistance of the BP/Ti₃C₂T_x-based sensor to acetone, ammonia, ethanol, and ether. It could be seen that the change in the resistance of BP/Ti₃C₂T_x in the presence of light was higher than that in the absence of light due to the fact that light promoted the electron exchange of gas molecules on the surface of BP/Ti₃C₂T_x. The resistance of the sensor increased in the target gas environment with or without light. This might be attributed to the electron transfer due to the adsorption of the gas molecules by the surface groups of BP/Ti₃C₂T_x, resulting in a decrease in the concentration of hole carriers inside BP/Ti₃C₂T_x. Notably, at 5 ppm, the response values of the BP/Ti₃C₂T_x-based sensors for acetone, ammonia, ether, and ethanol under light were 7.21%, 3.67%, 9.32%, and 7.55%, respectively, which were 1.19, 1.22, 1.26, and 1.07 times of the responses without light (Figs. 4e and S8a–c). This might be due to the photon excitation of BP/Ti₃C₂T_x surface electrons, which promoted the adsorption of gas molecules onto the material surface, thus reducing the carrier density in Ti₃C₂T_x and improving the sensitivity. When the gas concentration increased, the number of carriers decreased, and the channel resistance increased, thus increasing the sensor resistance.

Compared with the reported light-activated gas sensors, the BP/Ti₃C₂T_x gas sensor responded significantly to the target gas and exhibited excellent gas-sensitive performance (Table S1). In addition, to visualize the relationship between the target gas concentration and the sensor response, the natural logarithm of the response values of the BP/Ti₃C₂T_x-based sensors in the presence and absence of light was linearly fitted to the natural logarithm of the gas concentration. As shown in Figs. 4f and S9a–c, for acetone and ether, the slope in the presence of light was larger than that in the absence of light as the gas concentration increased. While the slope of ammonia and ethanol in the presence of light was less than that in the absence of light. The results showed that the BP/Ti₃C₂T_x based sensor was more sensitive to the gas of acetone and ether in the presence of light, which might be due to the stronger adsorption capacity of BP/Ti₃C₂T_x for them

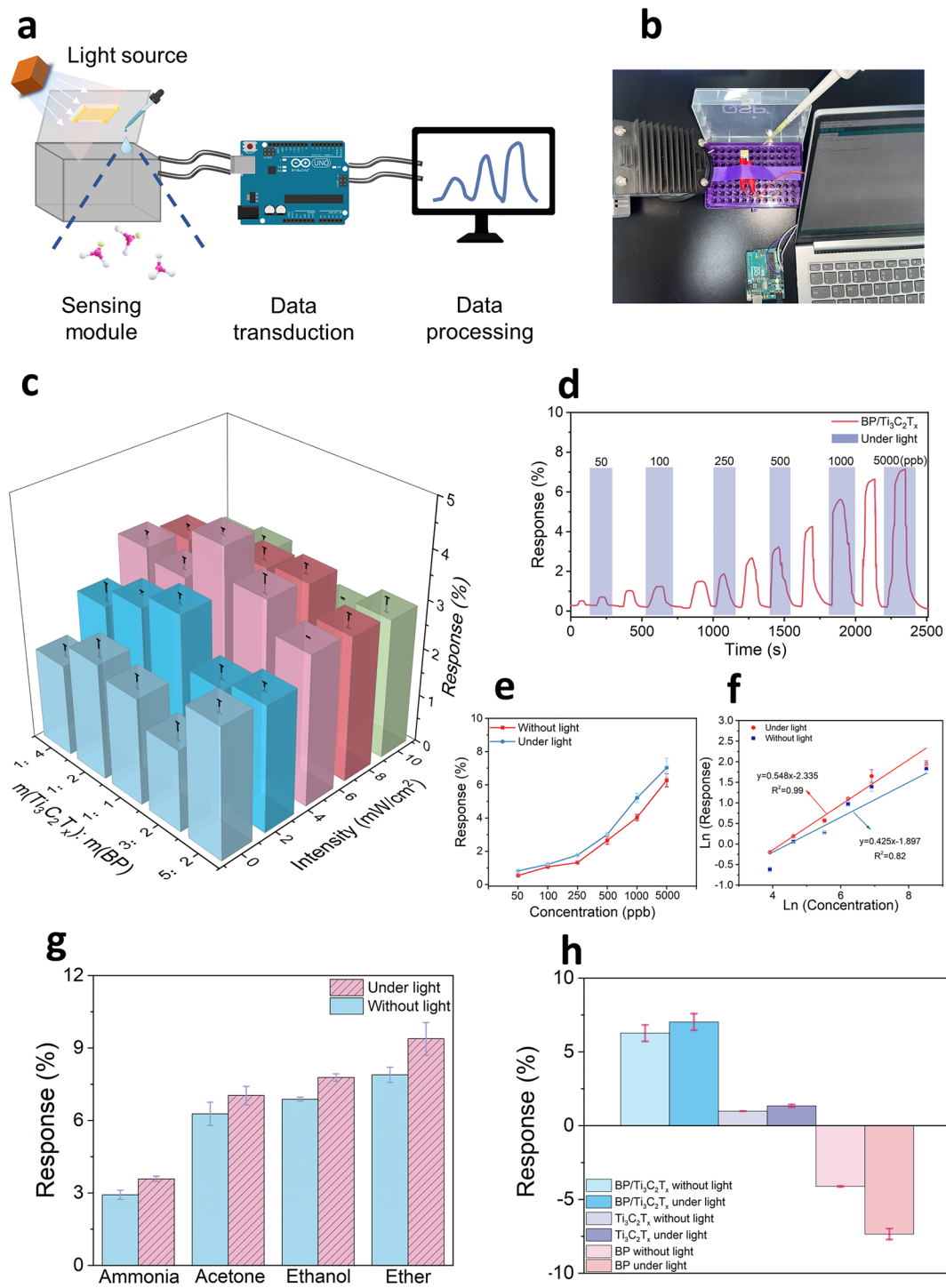


Fig. 4 Structure of IGSP and sensing performance of the BP/Ti₃C₂T_x composite. **a** Diagram of the working of LAVSA-based IGSP. Figures were created with BioRender. **b** Real picture of the sensing module. **c** Response of different ratios of BP/Ti₃C₂T_x composite at different light intensities at 420 nm to acetone at the concentration of 5 ppm. **d** Sensing performance of BP/Ti₃C₂T_x composite to acetone at concentrations from 50 ppb to 5 ppm in the presence and absence of light. **e** Comparison of the performance of the BP/Ti₃C₂T_x composite in the presence and absence of light to acetone at concentrations ranging from 50 ppb to 5 ppm. **f** Comparison of the logarithm linear relationship between the response and the acetone concentration of BP/Ti₃C₂T_x composite in the presence and absence of light. **g** Comparison of the performance of the BP/Ti₃C₂T_x composite in the presence and absence of light to ammonia, acetone, ethanol, and ether of 5 ppm. **h** Comparison of the response of the Ti₃C₂T_x, BP, and BP/Ti₃C₂T_x composite to acetone at the concentration of 5 ppm in the presence and absence of light

in the presence of light. Notably, the BP/Ti₃C₂T_x-based sensor showed good linearity for these gases in the range of 50 ppb to 5 ppm, suggesting that the sensor could be further practically applied for real-time monitoring and concentration measurement where the concentration range spanned 100-fold.

To compare the selectivity of BP/Ti₃C₂T_x in the presence and absence of light conditions, each of the above four gases was tested at 5 ppm. The results were shown in Fig. 4g, where the difference between the responses of the different gases became larger in the presence of light, indicating that the selectivity of the gases was improved. In addition, to compare the effect of light on the gas sensing performance of Ti₃C₂T_x, BP, and BP/Ti₃C₂T_x composites, the four gases were tested at 5 ppm with and without light conditions, respectively. The results were shown in Figs. 4h and S10a–c, where the three materials had responses of 1.13%, –4.03%, and 6.06% without light. In the presence of light, the corresponding responses were 1.07, 1.76, and 1.19 times higher, respectively, indicating that the light made the response differences between the sensors larger thus owning greater selectivity.

In a word, the response of BP/Ti₃C₂T_x to different gases was enhanced to varying degrees under light, resulting in greater variability in the gas response and thus improved selectivity. In addition, due to the nature of Ti₃C₂T_x itself and the synergistic effect with BP, its sensitivity remained high. This was important for detecting low concentration target gases in practical application scenarios. Therefore, the high sensitivity of BP/Ti₃C₂T_x under light made it a strong contender for gas sensors and could be further prepared with BP and Ti₃C₂T_x to form the LAVSA with excellent performance.

3.3 Sensing Characteristics of LAVSA

Previous studies on gas sensor arrays typically required testing a large number of different materials to obtain a single sensor with unique properties, and the marginal benefit decreased as the number of sensors was raised. Ti₃C₂T_x, BP, and BP/Ti₃C₂T_x themselves had large differences for gases, and photomodulation could increase this difference. In this work, inspired by the photomodulation strategy, if a SA made of these three materials detected gases in the presence and absence of light, which allowed for two times the

gas sensing data, and the dimensionality of the sensors was equivalent to doubling. The original SA consisted of three single sensors, and under light modulation, it was equivalent to introducing three virtual sensors to prepare the LAVSA. This not only simplified the preparation process of the SA, but also maintained the good performance. The LAVSA fabricated in this work consisted of six sensors, including Sensor 1: (without light) BP/Ti₃C₂T_x, Sensor 2: (under light) BP/Ti₃C₂T_x, Sensor 3: (without light) Ti₃C₂T_x, Sensor 4: (under light) Ti₃C₂T_x, Sensor 5: (without light) BP, and Sensor 6: (under light) BP.

First, the four gases mentioned above were detected to test the sensitivity performance of the LAVSA. The sensitivity of the LAVSA was tested by exposing it to a target gas environment ranging from 50 ppb to 5 ppm. After collecting the data, a pattern recognition algorithm was utilized to differentiate and identify the different gases (Fig. 5a, b). As shown in Fig. S11a–d, the response of each sensor was enhanced with increasing target gas concentration. Due to the different compositions of the sensors, they responded to gases to various degrees (Fig. 5c). For example, for 5 ppm ammonia, the response of sensor (with light) BP/Ti₃C₂T_x was 3.67%, while sensor (with light) BP was –11.03%. This difference could be used to demonstrate the selectivity of the LAVSA. Seven experiments were conducted for each of the four gases mentioned above at a concentration of 5 ppm, and the data were analyzed using principal component analysis (PCA) [67]. Figure 5d shows that the various gases clustered in a corresponding region, indicating that the LAVSA was able to differentiate between these gases at a concentration of 5 ppm, and therefore had excellent selectivity for these gases. This was mainly attributed to the selective accumulation of the six sensors in the LAVSA, which maximized the differentiation of the various gases by characterizing them in six dimensions. This indicated the successful fabrication of the LAVSA and demonstrated that it was constructed from individual sensors prepared with different ratios of BP to Ti₃C₂T_x. It had remarkable results in selectively recognizing the target gases under light modulation.

To test the actual performance of the LAVSA, 15 odor molecules (Table S2) were introduced and tested accordingly, choosing a total of five categories of substances, i.e., alcohols, ketones, aldehydes, esters, and acids. These molecules were widely found in nature and were therefore typical (Fig. S13). The LAVSA was exposed to 15 different

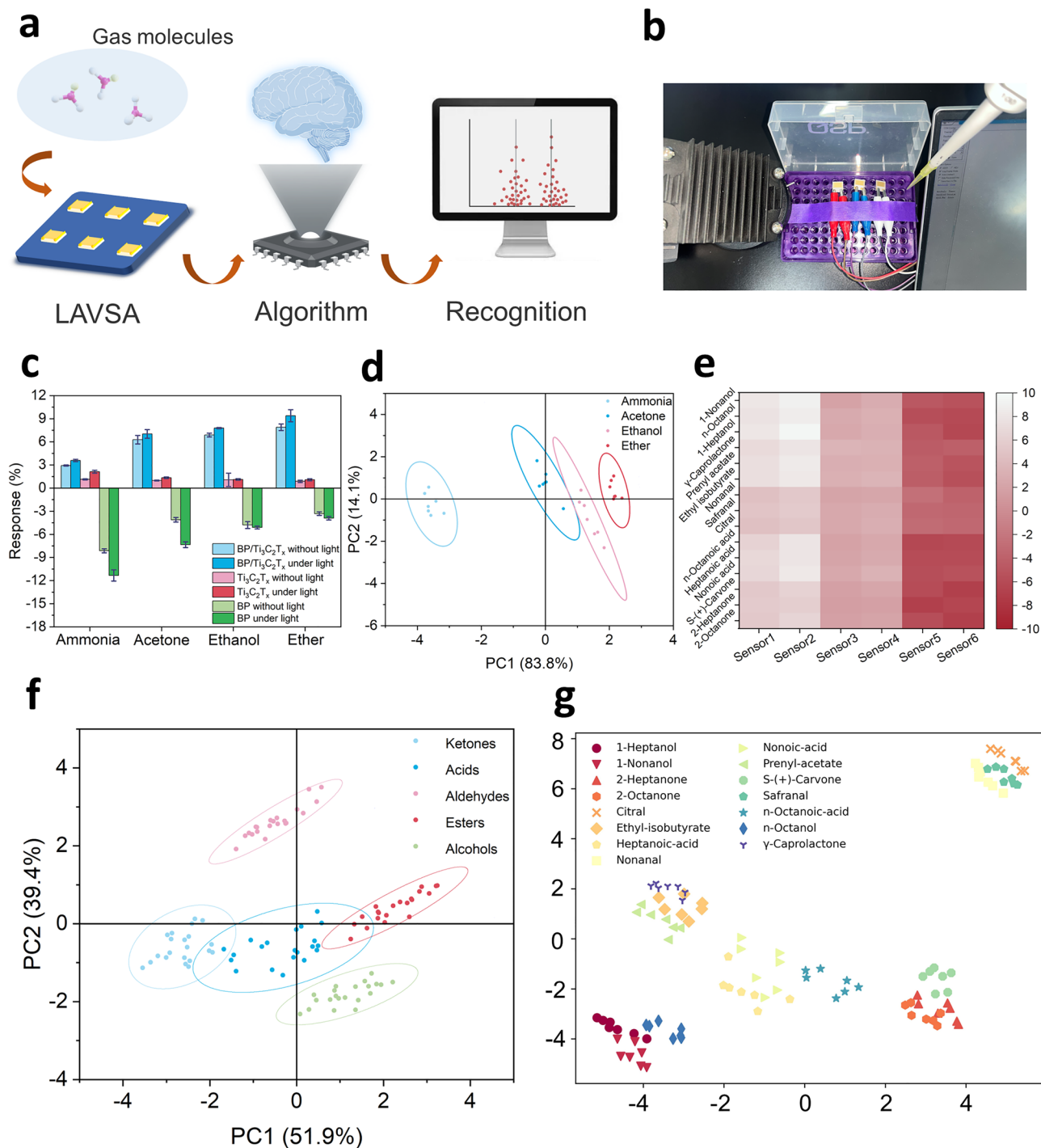


Fig. 5 Gas sensing performance of the LAVSA. **a** Diagram of the working of the LAVSA. Figures were created with BioRender. **b** Real picture of the LAVSA. **c** Gas sensing performance of the LAVSA exposed to ammonia, acetone, ethanol and ether of 5 ppm. **d** Image of PCA of the LAVSA to ammonia, acetone, ethanol, and ether of 5 ppm. **e** Average sensing performance of individual sensor in LAVSA to fifteen natural gas molecules of 5 ppm. **f** Image of PCA of the LAVSA to five types of natural gas molecules of 5 ppm. **g** Image of t-SNE of the LAVSA to fifteen natural gas molecules of 5 ppm

gases from 50 ppb to 5 ppm to monitor their performance (Fig. S12a–o). Each sensor had a different average performance value for each gas (Fig. 5e), which demonstrated the selective performance of the LAVSA. Seven experiments were then conducted for each of these gases at a concentration of 5 ppm, and the data obtained were analyzed with the help of PCA. Due to the apparent differences in the functional groups of these five types of odor molecules, it could be seen that each type of gas molecule was clustered in the corresponding region, showing a good clustering feature, indicating that the LAVSA was capable of classifying these five types of gas molecules with the help of PCA (Fig. 5f).

In addition, a new algorithm t-distributed stochastic neighborhood embedding (t-SNE) method was introduced to distinguish these 15 gas molecules [68]. After extracting the features from the sensor data and dimensionality reduction, a t-SNE plot (Fig. 5g) was drawn, with the values of the axes representing the differences in the features of different gases. As could be seen in the graph, the 15 gases were clustered separately and were clearly distinguishable. The results showed that with the assistance of the t-SNE algorithm and the PCA algorithm, the LAVSA had excellent sensitivity and selectivity, and could accurately identify both the five types of odor molecules and the 15 specific gases. In conclusion, the testing of the 15 odor molecules showed that the LAVSA consisting of BP and $Ti_3C_2T_x$ had excellent sensitivity and selectivity, and had the capability for further practical applications.

3.4 CHD Patient Identification on LAVAS-Based IGSP

Gas sensing had great potential for healthcare applications such as disease diagnosis. In this work, the detection and diagnosis of CHD patients by LAVSA-based IGSP with the help of an ML algorithm was explored (Fig. 6a). The diagnostic criteria for CHD was usually the degree of coronary artery stenosis (CAS), where 0–25% was considered mild, 25–50% was considered moderate, as well as greater than 50% was considered severe, and when the degree of CAS was greater than 50% it could be adjudged to be suffering from CHD [69, 70]. The rationale for non-invasive diagnosis through exhaled breath was that the body's exhaled gas encompassed its unique metabolic profile. Therefore, the composition of exhaled gas in patients with varying

degrees of CAS might differ from that of exhaled gas in healthy individuals. Multidimensional feature signals could be collected by IGSP and classified with the help of various mathematical algorithms. Since exhaled breath consisted of various components, depending on the biomarkers in it, each person had their own unique signals, and the LAVSA could detect these electrical signals and further differentiate them with the help of ML algorithms. The experiment was designed with a total of 45 participants (Table S3), including 10 healthy individuals (H), 11 patients with degree of CAS 0–25% (CAS-1), 9 patients with degree of CAS 25%–50% (CAS-2), and 15 patients with degree of CAS more than 50% (CAS-3).

The complexity of odor components in the exhaled gas and the differences in exhaled gas odor components between patients with different degrees of CAS and the healthy population was the basis for identification and classification. The samples from H, CAS-1, CAS-2, and CAS-3, were subjected to gas chromatography-mass spectrometry (GC–MS) to determine the differences in the odor components of exhaled gases in different populations, respectively. The GC–MS results (Fig. S14) visually showed that there were some differences in exhaled odors among different categories of people. Analyzed and further summarized, as shown in Tables S4–S7, the H samples contained components of ethyl acetate, acetone, and 2-ethyl-1-hexanol and so on. The CAS-1 samples contained components of 2,2,4-trimethyl-1,3-pentanediol diisobutyrate, acetone, ethyl acetate, etc. The CAS-2 samples contained components of 2-ethyl-1-hexanol, acetone, ethyl acetate, and so on. The CAS-3 samples contained components of acetone, ethyl acetate, ethanol, and so on. The diversity of compositions indicated that the biomarkers contained in the different types of samples were clearly recognizable.

In this work, the IGSP was utilized with the assistance of ML algorithms to process odor data exhaled by different volunteers and identify exhaled gases with unique sample categories. Samples were first collected via a sealed gas bag with a volume of 1 L, then the sample gas was placed 2 cm above the LAVSA (Fig. 6b), and the sample bag was gently pressed. The test was repeated 20 times for each sample. The data size was 45 people \times 20 experiments, which meant 900 sets of data were obtained. In terms of the performance of the gas detection platform, the mean response (Fig. 6g) showed that the gas detection platform responded

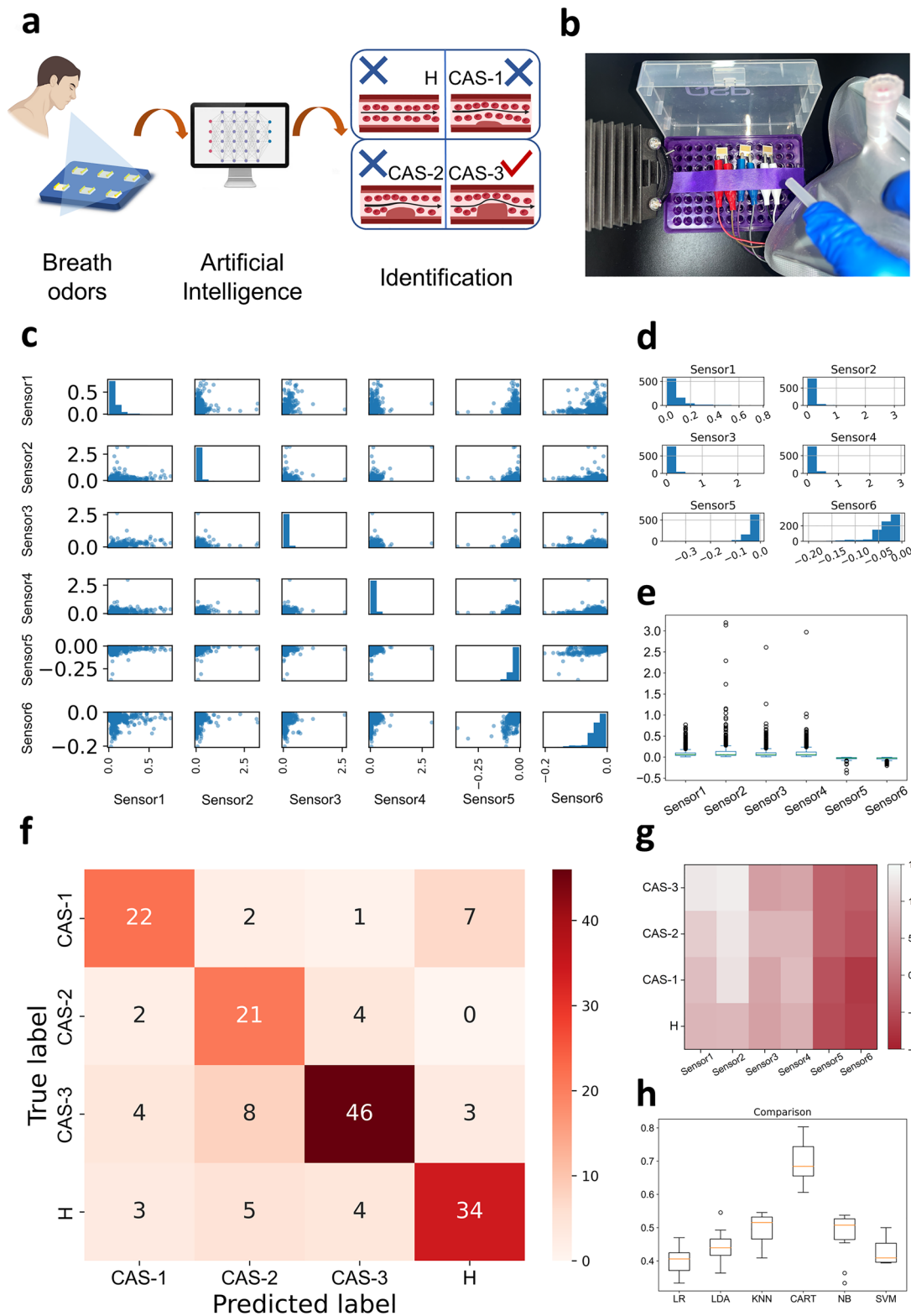


Fig. 6 Illustration and outcome of CHD recognition via breath odors. **a** Diagram of the disease recognition with IGSP, **b** Real picture of the IGSP on testing breath odors. Statistical graphics of **c** Scatter matrix, **d** Histogram, and **e** Box plot of the performance of individual sensors in LAVSA to breath odors. **f** Results of the confusion matrix for recognizing four types of volunteers, including H, CAS-1, CAS-2, and CAS-3. **g** Average performance of the IGSP to breath odors. **h** Comparison of the accuracy of six types of ML algorithms recognizing different types of volunteers via breath odors. Figures were created with BioRender

significantly to all four types of breath samples. In terms of the selectivity of the gas detection platform, the IGSP responded differently to each category of volunteer exhaled gas based on the various compositions of different categories of exhaled gas samples.

To detect and identify gas samples through the IGSP, ML algorithms were utilized to help achieve this. First, the data had to be pre-processed by organizing it into a size of 20×45 and further classified into four labels according to four categories. The data was then used for algorithm training and optimization. The histogram (Fig. 6d) and the boxplot diagram (Fig. 6e) showed the distribution of gas sensing performance of individual sensors in the LAVSA, showing the diversity of responses to various types of gas samples. The mathematical relationships between the sensors were shown in a scatter matrix plot (Fig. 6c), indicating significant differences between the signals. Six ML algorithms were used for data processing, namely logistic regression (LR), linear discriminant analysis (LDA), K-Nearest Neighbor algorithm (KNN), classification and regression tree (CART), Naive Bayes model (NB), and support vector machine (SVM) [33, 71–77]. From the confusion matrix (Fig. 6f), it could be seen that for the four categories of participants from different populations, H was predicted with 77% accuracy, CAS-1 predicted with 71% accuracy, CAS-2 predicted with 58% accuracy, and CAS-3 with 84% accuracy. Figure 6h showed the prediction results of the six algorithms through 10 cross-validation tests. CART had the best performance with an accuracy of 0.692, which meant that it performed well in recognizing breath odors. In comparison, LR had an accuracy of 0.403, which proved that it was not suitable for inter-sample identification. However, the IGSP had some limitations, such as it required known calibration samples for comparison to achieve accurate detection, which required an extensive library of calibration samples, and the detection of unrecorded gas categories remained an open issue. Also, determining the composition and corresponding concentration of exhaled gases through the IGSP remained challenging.

3.5 IGSP Sensing Mechanism

The gas-sensitizing properties of BP/Ti₃C₂T_x nanocomplexes were enhanced under visible light irradiation compared to pristine Ti₃C₂T_x (Fig. 7a). This was mainly due

to the synergistic effect between BP and Ti₃C₂T_x, as well as the increased electron exchange due to photon activation. On the one hand, the self-growth of BP nanosheets could lead to higher specific surface area and active sites, which resulted in enhanced gas adsorption and desorption processes. On the other hand, the heterostructure formed by BP and Ti₃C₂T_x, as well as the modulation of carrier density through photon excitation, were important factors to improve the gas-sensitive performance of the sensor. According to the literature, the conduction band (CB) potential and valence band (VB) potential of BP were 0.83 and 1.17 eV, respectively [78]. Under visible light irradiation, photo-excited electrons were transferred from the VB to the CB of the BP. Because of the lower Fermi energy level (E_F) equal to -0.17 eV of Ti₃C₂T_x, the electrons would be further transferred to Ti₃C₂T_x [79]. Since the E_F of Ti₃C₂T_x was more negative than the potential of O₂/O₂⁻ equal to 0.046 eV and Ti₃C₂T_x had excellent conductivity (4600 ± 1100 S cm⁻¹), the acquired photogenerated electrons were rapidly transferred to the surface of Ti₃C₂T_x and eventually captured by O₂ [78, 80, 81]. Gas molecules such as VOCs absorbed O₂⁻ electrons on the surface of Ti₃C₂T_x to generate CO₂ and H₂O. Therefore, the electron exchange between the target gas and the surface of the BP/Ti₃C₂T_x was enhanced through the above process. In all, the enhanced gas sensitivity performance of the BP/Ti₃C₂T_x-based sensor was attributed to the formation of heterogeneous structure, the increase of active site, and photomodulated carrier density.

The improved gas sensing performance of the prepared IGSP could be attributed to three main factors (Fig. 7b). First, the construction of BP/Ti₃C₂T_x heterostructured complexes capable of photoresponsiveness provided a rich material base for high-performance gas sensing and facilitated the development of LAVSA. Second, the LAVSA consisted of three BP/Ti₃C₂T_x with different compositions, which operated under the presence and absence of light conditions, thus enabling the acquisition of multidimensional data to improve the characterization of the target gas and facilitating data collection and processing by combining with pattern recognition algorithms. Finally, with the help of ML algorithms, the data obtained by LAVSA could improve the differentiation of target gas characteristics. Comparative analysis of multiple ML algorithms allowed training on known samples, thus selecting the most accurate model for determining

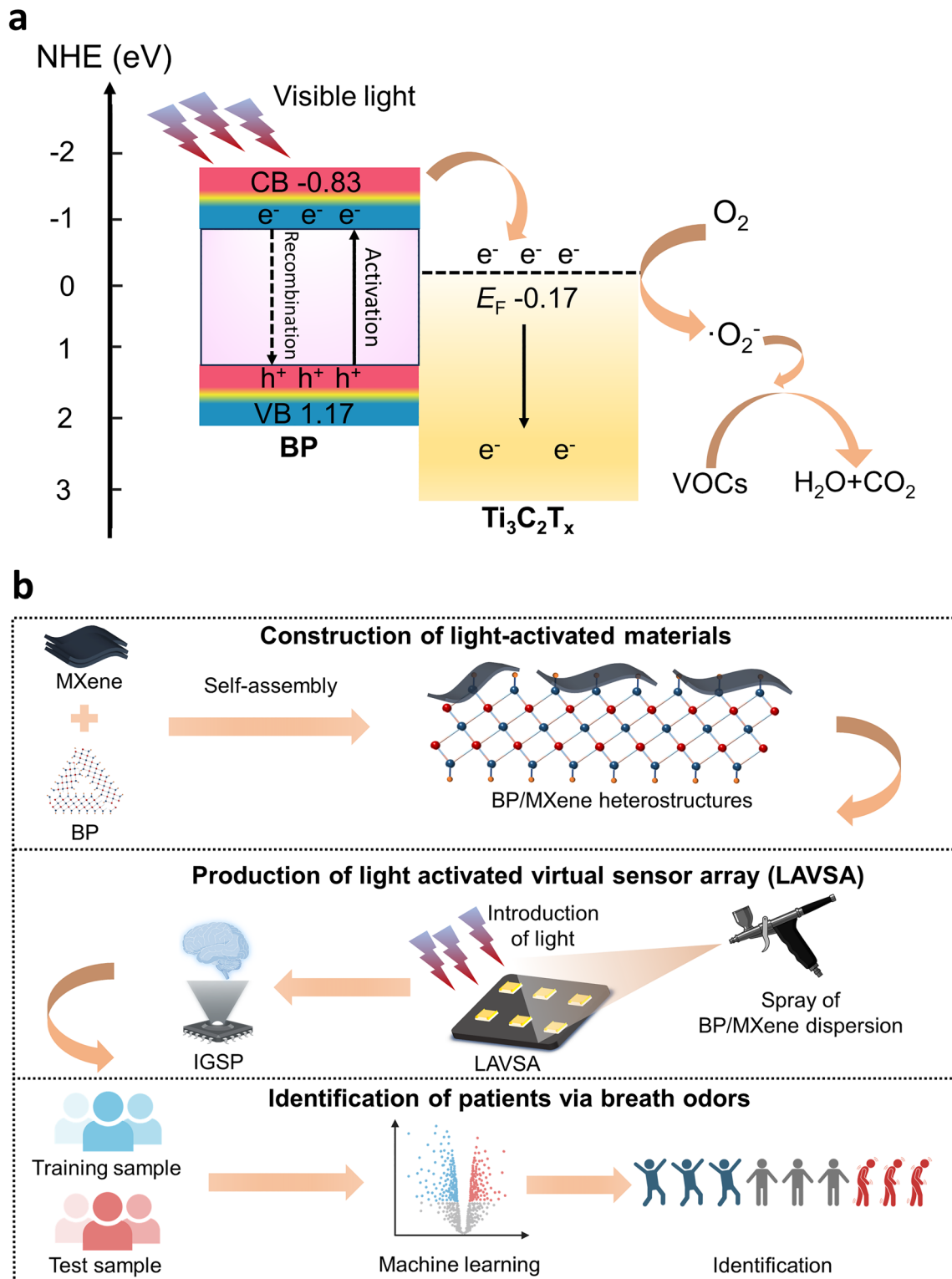


Fig. 7 The mechanism of enhanced sensing property of the IGSP. **a** Change of conductivity pathway of the BP/Ti₃C₂T_x gas sensor after adsorption due to light activation. **b** Diagram of the improved sensing performance of the fabricated IGSP in disease recognition. Figures were created with BioRender

sample attribution. In conclusion, through improved material screening and preparation, data collection, and processing, the IGSP demonstrated excellent performance in gas detection and identification.

4 Conclusions

In summary, the goal of the research was to establish an LAVSA and IGSP for the identification of different populations by human odor and for non-invasive diagnosis of CHD. In this work, from the perspective of photomodulation, BP was screened from materials whose light absorption range overlapped with that of MXene, and the BP/Ti₃C₂T_x complex was synthesized with MXene using a self-assembly strategy. As a proof-of-concept, sensors were fabricated using BP/Ti₃C₂T_x and tested against ammonia, acetone, ethanol, and ether gases to determine the optimal values of light wavelength and intensity as well as material ratios. Due to the synergistic effect of BP and MXene as well as photoexcitation, the complexes showed higher gas-sensitive performance, with a 26% higher response under light than in the absence of light, as well as an improvement in selectivity. On this basis, LAVSA was prepared using three different ratios of BP/Ti₃C₂T_x materials and tested for fifteen odor molecules under light and no light conditions, respectively. The recognition and classification of different gases were successfully realized with the help of PCA and t-SNE pattern recognition algorithms, which demonstrated its selectivity. Finally, the IGSP fabricated based on LAVSA and Arduino platform was put to practical use, and 45 volunteers were selected for testing, including healthy people and patients with three different degrees of CAS. With the help of the ML algorithm, the IGSP achieved an accuracy of 77%, 71%, 58%, and 84% in recognizing four different populations, H, CAS-1, CAS-2, and CAS-3, respectively, by human breath, and showed good recognition performance in both CAS patients and healthy people.

Inspired by physical modulation, the concept of LAVSA was proposed, and the BP/Ti₃C₂T_x complexes were fabricated, providing a new approach for the development of novel gas sensors with high sensitivity and selectivity. Besides, the IGSP fabricated in this study provided ideas for non-invasive diagnosis of CHD and also offered ideal prospects for immediate detection and identification of

other diseases, such as tumors, as well as other applications in immediate gas sensing scenarios. Despite the good performance of the prepared IGSP, it still faces challenges in practical applications, which are what future research needs to focus on. On the one hand, the responsiveness of LAVSA still needs to be improved. On the other hand, the current training database was small in size and had limitations in large-scale applications. To settle these problems, there are three areas that can be addressed in future research. First, in terms of material and SA design, light-responsive materials could be further screened. Better-structured materials could be designed and synthesized to enhance the sensitivity. Besides, the wavelength and lightness of light and time could be further optimized to improve the accuracy and sensitivity. Second, regarding data collection, more data is needed to increase the stability of the IGSP. In future studies, gases from more scenarios will be detected, such as exhaled gas samples from lung cancer patients and stomach cancer patients. By collecting more data, a large database will be constructed for more applications. Finally, regarding data processing, more accurate ML algorithms need to be designed. The machine learning algorithms used in the current study leave much to be desired in terms of accuracy. In future research, on the one hand, the accuracy of the ML algorithm model is trained by collecting more data. On the other hand, it is to enhance the discriminative ability by improving the ML algorithm, such as adopting neural networks.

Acknowledgements This work was supported by the National Natural Science Foundation of China (22278241), the National Key R&D Program of China (2018YFA0901700), a grant from the Institute Guo Qiang, Tsinghua University (2021GQG1016), and Department of Chemical Engineering-iBHE Joint Cooperation Fund.

Declarations

Conflict of interest The authors declare no interest conflict. They have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

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Supplementary Information The online version contains supplementary material available at <https://doi.org/10.1007/s40820-024-01481-7>.

References

- S. Coffey, R. Roberts-Thomson, A. Brown, J. Carapetis, M. Chen et al., Global epidemiology of valvular heart disease. *Nat. Rev. Cardiol.* **18**, 853–864 (2021). <https://doi.org/10.1038/s41569-021-00570-z>
- M.A. Khan, M.J. Hashim, H. Mustafa, M.Y. Baniyas, S.K.B.M. Al Suwaidi et al., Global epidemiology of ischemic heart disease: results from the global burden of disease study. *Cureus* **12**, e9349 (2020). <https://doi.org/10.7759/cureus.9349>
- N.F. Narvaez Linares, M. Poitras, J. Burkauskas, K. Nagaratanam, Z. Burr et al., Neuropsychological sequelae of coronary heart disease in women: a systematic review. *Neurosci. Biobehav. Rev.* **127**, 837–851 (2021). <https://doi.org/10.1016/j.neubiorev.2021.05.026>
- J.A. Ladapo, S. Blecker, P.S. Douglas, Physician decision making and trends in the use of cardiac stress testing in the United States: an analysis of repeated cross-sectional data. *Ann. Intern. Med.* **161**, 482–490 (2014). <https://doi.org/10.7326/M14-0296>
- T. Ikeda, Current use and future needs of noninvasive ambulatory electrocardiogram monitoring. *Intern. Med.* **60**, 9–14 (2021). <https://doi.org/10.2169/internalmedicine.5691-20>
- U. Hoffmann, M. Ferencik, R.C. Cury, A.J. Pena, Coronary CT angiography. *J. Am. Coll. Radiol.* **3**, 560–564 (2006). <https://doi.org/10.1016/j.jacr.2006.02.034>
- J. Limeres, J.F. Garcez, J.S. Marinho, A. Loureiro, M. Diniz et al., A breath ammonia analyser for monitoring patients with end-stage renal disease on haemodialysis. *Br. J. Biomed. Sci.* **74**, 24–29 (2017). <https://doi.org/10.1080/09674845.2016.1239886>
- T. Karl, P. Prazeller, D. Mayr, A. Jordan, J. Rieder et al., Human breath isoprene and its relation to blood cholesterol levels: new measurements and modeling. *J. Appl. Physiol.* **91**, 762–770 (2001). <https://doi.org/10.1152/jappl.2001.91.2.762>
- I. Nardi Agmon, Y.Y. Broza, G. Alaa, A. Eisen, A. Hamdan et al., Detecting coronary artery disease using exhaled breath analysis. *Cardiology* **147**, 389–397 (2022). <https://doi.org/10.1159/000525688>
- Y. Feng, J. Chang, X. Chen, Q. Zhang, Z. Wang et al., Application of TDM and FDM methods in TDLAS based multi-gas detection. *Opt. Quantum Electron.* **53**, 195 (2021). <https://doi.org/10.1007/s11082-021-02844-9>
- R.K. Jha, Non-dispersive infrared gas sensing technology: a review. *IEEE Sens. J.* **22**, 6–15 (2022). <https://doi.org/10.1109/JSEN.2021.3130034>
- W. Zhang, C. Zuo, T. Liao, G. Zhou, D. Zhao, Research on improving the performance of motor vehicle exhaust gas detection system based on DOAS technology. Ninth symposium on novel photoelectronic detection technology and applications. Hefei, China. SPIE, 2–4 Nov 2023 <https://doi.org/10.1117/12.2664361>
- S. Dhall, B.R. Mehta, A.K. Tyagi, K. Sood, A review on environmental gas sensors: Materials and technologies. *Sens. Int.* **2**, 100116 (2021). <https://doi.org/10.1016/j.sintl.2021.100116>
- I. Gaillard, S. Rouquier, D. Giorgi, Olfactory receptors. *Cell. Mol. Life Sci.* **61**, 456–469 (2004). <https://doi.org/10.1007/s00018-003-3273-7>
- L.B. Buck, Olfactory receptors and odor coding in mammals. *Nutr. Rev.* **62**, S184–S188 (2004). <https://doi.org/10.1111/j.1753-4887.2004.tb00097.x>
- C. Qin, Y. Wang, J. Hu, T. Wang, D. Liu et al., Artificial olfactory biohybrid system: an evolving sense of smell. *Adv. Sci.* **10**, e2204726 (2023). <https://doi.org/10.1002/advs.202204726>
- D. Pan, J. Hu, B. Wang, X. Xia, Y. Cheng et al., Biomimetic wearable sensors: emerging combination of intelligence and electronics. *Adv. Sci.* **11**, e2303264 (2024). <https://doi.org/10.1002/advs.202303264>
- A. Solórzano, J. Eichmann, L. Fernández, B. Ziems, J.M. Jiménez-Soto et al., Early fire detection based on gas sensor arrays: Multivariate calibration and validation. *Sens. Actuat. B Chem.* **352**, 130961 (2022). <https://doi.org/10.1016/j.snb.2021.130961>
- M. Kang, I. Cho, J. Park, J. Jeong, K. Lee et al., High accuracy real-time multi-gas identification by a batch-uniform gas sensor array and deep learning algorithm. *ACS Sens.* **7**, 430–440 (2022). <https://doi.org/10.1021/acssensors.1c01204>
- S. Herberger, M. Herold, H. Ulmer, A. Burdack-Freitag, F. Mayer, Detection of human effluents by a MOS gas sensor in correlation to VOC quantification by GC/MS. *Build. Environ.* **45**, 2430–2439 (2010). <https://doi.org/10.1016/j.buildenv.2010.05.005>
- S. Das, V. Jayaraman, SnO₂: a comprehensive review on structures and gas sensors. *Prog. Mater. Sci.* **66**, 112–255 (2014). <https://doi.org/10.1016/j.pmatsci.2014.06.003>
- P. Samarasekera, N.N. Kumara, N.S. Yapa, Sputtered copper oxide (CuO) thin films for gas sensor devices. *J. Phys. Condens. Matter* **18**, 2417–2420 (2006). <https://doi.org/10.1088/0953-8984/18/8/007>
- J. Zhang, Z. Qin, D. Zeng, C. Xie, Metal-oxide-semiconductor based gas sensors: screening, preparation, and integration. *Phys. Chem. Chem. Phys.* **19**, 6313–6329 (2017). <https://doi.org/10.1039/c6cp07799d>
- A. Trinchi, S. Kandasamy, W. Wlodarski, High temperature field effect hydrogen and hydrocarbon gas sensors based on



- SiC MOS devices. *Sens. Actuat. B Chem.* **133**, 705–716 (2008). <https://doi.org/10.1016/j.snb.2008.03.011>
25. Y. Yan, G. Yang, J.-L. Xu, M. Zhang, C.-C. Kuo et al., Conducting polymer-inorganic nanocomposite-based gas sensors: a review. *Sci. Technol. Adv. Mater.* **21**, 768–786 (2020). <https://doi.org/10.1080/14686996.2020.1820845>
26. P.V. Shinde, A. Patra, C.S. Rout, A review on the sensing mechanisms and recent developments on metal halide-based perovskite gas sensors. *J. Mater. Chem. C* **10**, 10196–10223 (2022). <https://doi.org/10.1039/d2tc01980a>
27. K.R.G. Lim, M. Shekhirev, B.C. Wyatt, B. Anasori, Y. Gogotsi et al., Fundamentals of MXene synthesis. *Nat. Synth* **1**, 601–614 (2022). <https://doi.org/10.1038/s44160-022-00104-6>
28. S.J. Kim, H.J. Koh, C.E. Ren, O. Kwon, K. Maleski et al., Metallic $Ti_3C_2T_x$ MXene gas sensors with ultrahigh signal-to-noise ratio. *ACS Nano* **12**, 986–993 (2018). <https://doi.org/10.1021/acsnano.7b07460>
29. J.-C. Lei, X. Zhang, Z. Zhou, Recent advances in MXene: preparation, properties, and applications. *Front. Phys.* **10**, 276–286 (2015). <https://doi.org/10.1007/s11467-015-0493-x>
30. X. Zhan, C. Si, J. Zhou, Z. Sun, MXene and MXene-based composites: synthesis, properties and environment-related applications. *Nanoscale Horiz.* **5**, 235–258 (2020). <https://doi.org/10.1039/C9NH00571D>
31. H. Yu, Y. Wang, Y. Jing, J. Ma, C.-F. Du et al., Surface modified MXene-based nanocomposites for electrochemical energy conversion and storage. *Small* **15**, e1901503 (2019). <https://doi.org/10.1002/sml.201901503>
32. X. Bai, J. Guan, MXenes for electrocatalysis applications: Modification and hybridization. *Chin. J. Catal.* **43**, 2057–2090 (2022). [https://doi.org/10.1016/s1872-2067\(21\)64030-5](https://doi.org/10.1016/s1872-2067(21)64030-5)
33. J. Hu, D. Liu, X. Xia, B. Wang, D. Pan et al., MXene/perovskite-based bionic human odor sensor array with machine learning. *Chem. Eng. J.* **468**, 143752 (2023). <https://doi.org/10.1016/j.cej.2023.143752>
34. S. Sun, M. Wang, X. Chang, Y. Jiang, D. Zhang et al., $W_{18}O_{49}/Ti_3C_2T_x$ MXene nanocomposites for highly sensitive acetone gas sensor with low detection limit. *Sens. Actuat. B Chem.* **304**, 127274 (2020). <https://doi.org/10.1016/j.snb.2019.127274>
35. F. Xu, H.-P. Ho, Light-activated metal oxide gas sensors: a review. *Micromachines* **8**, 333 (2017). <https://doi.org/10.3390/mi8110333>
36. J. Wang, H. Shen, Y. Xia, S. Komarneni, Light-activated room-temperature gas sensors based on metal oxide nanostructures: a review on recent advances. *Ceram. Int.* **47**, 7353–7368 (2021). <https://doi.org/10.1016/j.ceramint.2020.11.187>
37. I. Karaduman, D.E. Yildiz, M.M. Sincar, S. Acar, UV light activated gas sensor for NO_2 detection. *Mater. Sci. Semicond. Process.* **28**, 43–47 (2014). <https://doi.org/10.1016/j.mssp.2014.04.011>
38. H. Tabata, H. Matsuyama, T. Goto, O. Kubo, M. Katayama, Visible-light-activated response originating from carrier-mobility modulation of NO_2 gas sensors based on MoS_2 monolayers. *ACS Nano* **15**, 2542–2553 (2021). <https://doi.org/10.1021/acsnano.0c06996>
39. R. Li, L. Zhang, L. Shi, P. Wang, MXene Ti_3C_2 : an effective 2D light-to-heat conversion material. *ACS Nano* **11**, 3752–3759 (2017). <https://doi.org/10.1021/acsnano.6b08415>
40. Q. Zhang, L. Yan, M. Yang, G. Wu, M. Hu et al., Ultrafast transient spectra and dynamics of MXene ($Ti_3C_2T_x$) in response to light excitations of various wavelengths. *J. Phys. Chem. C* **124**, 6441–6447 (2020). <https://doi.org/10.1021/acs.jpcc.9b11652>
41. X. Wang, S. Lan, Optical properties of black phosphorus. *Adv. Opt. Photon.* **8**, 618 (2016). <https://doi.org/10.1364/aop.8.000618>
42. M. Luo, T. Fan, Y. Zhou, H. Zhang, L. Mei, 2D black phosphorus-based biomedical applications. *Adv. Funct. Mater.* **29**, 1808306 (2019). <https://doi.org/10.1002/adfm.201808306>
43. A. Castellanos-Gomez, L. Vicarelli, E. Prada, J.O. Island, K.L. Narasimha-Acharya et al., Isolation and characterization of few-layer black phosphorus. *2D Mater.* **1**, 025001 (2014). <https://doi.org/10.1088/2053-1583/1/2/025001>
44. A. Garavand, C. Salehnasab, A. Behmanesh, N. Aslani, A.H. Zadeh et al., Efficient model for coronary artery disease diagnosis: a comparative study of several machine learning algorithms. *J. Healthc. Eng.* **2022**, 5359540 (2022). <https://doi.org/10.1155/2022/5359540>
45. A. Gupta, J.J. Slater, D. Boyne, N. Mitsakakis, A. Béliveau et al., Probabilistic graphical modeling for estimating risk of coronary artery disease: applications of a flexible machine-learning method. *Med. Decis. Making* **39**, 1032–1044 (2019). <https://doi.org/10.1177/0272989X19879095>
46. J.H. Joloudari, E. Hassannataj Joloudari, H. Saadatfar, M. Ghasemigol, S.M. Razavi et al., Coronary artery disease diagnosis: ranking the significant features using a random trees model. *Int. J. Environ. Res. Public Health* **17**, 731 (2020). <https://doi.org/10.3390/ijerph17030731>
47. Q. Zhang, H. Lai, R. Fan, P. Ji, X. Fu et al., High concentration of $Ti_3C_2T_x$ MXene in organic solvent. *ACS Nano* **15**, 5249–5262 (2021). <https://doi.org/10.1021/acsnano.0c10671>
48. Y. Guo, X. Zhou, D. Wang, X. Xu, Q. Xu, Nanomechanical properties of Ti_3C_2 MXene. *Langmuir* **35**, 14481–14485 (2019). <https://doi.org/10.1021/acs.langmuir.9b02619>
49. L. Li, Y. Yu, G.J. Ye, Q. Ge, X. Ou et al., Black phosphorus field-effect transistors. *Nat. Nanotechnol.* **9**, 372–377 (2014). <https://doi.org/10.1038/nnano.2014.35>
50. J. Tao, W. Shen, S. Wu, L. Liu, Z. Feng et al., Mechanical and electrical anisotropy of few-layer black phosphorus. *ACS Nano* **9**, 11362–11370 (2015). <https://doi.org/10.1021/acsnano.5b05151>
51. D. Yang, C. Zhao, R. Lian, L. Yang, Y. Wang et al., Mechanisms of the planar growth of lithium metal enabled by the 2D lattice confinement from a $Ti_3C_2T_x$ MXene intermediate layer. *Adv. Funct. Mater.* **31**, 2010987 (2021). <https://doi.org/10.1002/adfm.202010987>

52. S.H. Aldave, M.N. Yogeesh, W. Zhu, J. Kim, S.S. Sonde et al., Characterization and sonochemical synthesis of black phosphorus from red phosphorus. *2D Mater.* **3**, 014007 (2016). <https://doi.org/10.1088/2053-1583/3/1/014007>
53. Z. Sofer, D. Bouša, J. Luxa, V. Mazanek, M. Pumera, Few-layer black phosphorus nanoparticles. *Chem. Commun.* **52**, 1563–1566 (2016). <https://doi.org/10.1039/c5cc09150k>
54. Z. Lin, P. Rozier, B. Duployer, P.-L. Taberna, B. Anasori et al., Electrochemical and *in situ* X-ray diffraction studies of $Ti_3C_2T_x$ MXene in ionic liquid electrolyte. *Electrochem. Commun.* **72**, 50–53 (2016). <https://doi.org/10.1016/j.elecom.2016.08.023>
55. C.E. Shuck, A. Sarycheva, M. Anayee, A. Levitt, Y. Zhu et al., Scalable synthesis of $Ti_3C_2T_x$ MXene. *Adv. Engin. Mater.* **22**, 1901241 (2020). <https://doi.org/10.1002/adem.201901241>
56. L.-Å. Näslund, I. Persson, XPS spectra curve fittings of $Ti_3C_2T_x$ based on first principles thinking. *Appl. Surf. Sci.* **593**, 153442 (2022). <https://doi.org/10.1016/j.apsusc.2022.153442>
57. Y. Lu, D. Li, F. Liu, Characterizing the chemical structure of $Ti_3C_2T_x$ MXene by angle-resolved XPS combined with Argon ion etching. *Materials* **15**, 307 (2022). <https://doi.org/10.3390/ma15010307>
58. A. Ambrosi, Z. Sofer, M. Pumera, Electrochemical exfoliation of layered black phosphorus into phosphorene. *Angew. Chem. Int. Ed.* **56**, 10443–10445 (2017). <https://doi.org/10.1002/anie.201705071>
59. H. Asahina, A. Morita, Band structure and optical properties of black phosphorus. *J. Phys. C Solid State Phys.* **17**, 1839–1852 (1984). <https://doi.org/10.1088/0022-3719/17/11/006>
60. Y. Jiang, T. Sun, X. Xie, W. Jiang, J. Li et al., Oxygen-functionalized ultrathin $Ti_3C_2T_x$ MXene for enhanced electrocatalytic hydrogen evolution. *Chemsuschem* **12**, 1368–1373 (2019). <https://doi.org/10.1002/cssc.201803032>
61. W. Eom, H. Shin, T.H. Han, Tracking the thermal dynamics of $Ti_3C_2T_x$ MXene with XPS and two-dimensional correlation spectroscopy. *Appl. Phys. Lett.* **122**, 211601 (2023). <https://doi.org/10.1063/5.0143298>
62. Y. Geng, Y. Zhao, Y. Zhao, J. Feng, J. Zhang et al., Multifunctional organic single-crystalline microwire arrays toward optical applications. *Adv. Funct. Mater.* **32**, 2113025 (2022). <https://doi.org/10.1002/adfm.202113025>
63. Y.-J. Yuan, P. Wang, Z. Li, Y. Wu, W. Bai et al., The role of bandgap and interface in enhancing photocatalytic H_2 generation activity of 2D–2D black phosphorus/ MoS_2 photocatalyst. *Appl. Catal. B Environ.* **242**, 1–8 (2019). <https://doi.org/10.1016/j.apcatb.2018.09.100>
64. K. Wang, B.M. Szydłowska, G. Wang, X. Zhang, J.J. Wang et al., Ultrafast nonlinear excitation dynamics of black phosphorus nanosheets from visible to mid-infrared. *ACS Nano* **10**, 6923–6932 (2016). <https://doi.org/10.1021/acsnano.6b02770>
65. X. Jiang, S. Liu, W. Liang, S. Luo, Z. He et al., Broadband nonlinear photonics in few-layer Mxene $Ti_3C_2T_x$ ($t = F, O, \text{ or } OH$). *Laser Photonics Rev.* **12**, 1700229 (2018). <https://doi.org/10.1002/lpor.201870013>
66. T. Hou, Q. Li, Y. Zhang, W. Zhu, K. Yu et al., Near-infrared light-driven photofixation of nitrogen over $Ti_3C_2T_x/TiO_2$ hybrid structures with superior activity and stability. *Appl. Catal. B Environ.* **273**, 119072 (2020). <https://doi.org/10.1016/j.apcatb.2020.119072>
67. H. Ji, W. Qin, Z. Yuan, F. Meng, Qualitative and quantitative recognition method of drug-producing chemicals based on SnO_2 gas sensor with dynamic measurement and PCA weak separation. *Sens. Actuat. B Chem.* **348**, 130698 (2021). <https://doi.org/10.1016/j.snb.2021.130698>
68. P. Xu, K. Song, Y. Chen, G. Wei, Q. Wang, Fault diagnosis method of self-validating metal oxide semiconductor gas sensor based on t-distribution stochastic neighbor embedding and random forest. *Rev. Sci. Instrum.* **90**, 055002 (2019). <https://doi.org/10.1063/1.5090142>
69. J.M. Mann, M.J. Davies, Vulnerable plaque. Relation of characteristics to degree of stenosis in human coronary arteries. *Circulation* **94**, 928–931 (1996). <https://doi.org/10.1161/01.cir.94.5.928>
70. O.F. Donati, P. Stolzmann, L. Desbiolles, S. Leschka, S. Kozerke et al., Coronary artery disease: which degree of coronary artery stenosis is indicative of ischemia? *Eur. J. Radiol.* **80**, 120–126 (2011). <https://doi.org/10.1016/j.ejrad.2010.07.010>
71. S. Fan, Z. Li, K. Xia, D. Hao, Quantitative and qualitative analysis of multicomponent gas using sensor array. *Sensors* **19**, 3917 (2019). <https://doi.org/10.3390/s19183917>
72. U.N. Thakur, R. Bhardwaj, A. Hazra, Statistical analysis for selective identifications of VOCs by using surface functionalized MoS_2 based sensor array. The 1st international electronic conference on chemical sensors and analytical chemistry. Basel Switzerland, MDPI, (2021). <https://doi.org/10.3390/csac2021-10451>
73. Y. Yin, Y. Zhao, A feature selection strategy of E-nose data based on PCA coupled with Wilks Λ -statistic for discrimination of vinegar samples. *J. Food Meas. Charact.* **13**, 2406–2416 (2019). <https://doi.org/10.1007/s11694-019-00161-0>
74. T. Itoh, Y. Koyama, Y. Sakumura, T. Akamatsu, A. Tsuruta et al., Discrimination of volatile organic compounds using a sensor array via a rapid method based on linear discriminant analysis. *Sens. Actuat. B Chem.* **387**, 133803 (2023). <https://doi.org/10.1016/j.snb.2023.133803>
75. A. Boujnah, A. Boubaker, S. Pecqueur, K. Lmimouni, A. Kalboussi, An electronic nose using conductometric gas sensors based on P3HT doped with triflates for gas detection using computational techniques (PCA, LDA, and kNN). *J. Mater. Sci. Mater. Electron.* **33**, 27132–27146 (2022). <https://doi.org/10.1007/s10854-022-09376-2>
76. X. Zhao, P. Li, K. Xiao, X. Meng, L. Han et al., Sensor drift compensation based on the improved LSTM and SVM multi-class ensemble learning models. *Sensors* **19**, 3844 (2019). <https://doi.org/10.3390/s19183844>
77. M.A. Djeziri, O. Djedidi, N. Morati, J.-L. Seguin, M. Bendahan et al., A temporal-based SVM approach for the detection and identification of pollutant gases in a gas mixture.



- Appl. Intell. **52**, 6065–6078 (2022). <https://doi.org/10.1007/s10489-021-02761-0>
78. B. Shao, J. Wang, Z. Liu, G. Zeng, L. Tang et al., $\text{Ti}_3\text{C}_2\text{T}_x$ MXene decorated black phosphorus nanosheets with improved visible-light photocatalytic activity: experimental and theoretical studies. *J. Mater. Chem. A* **8**, 5171–5185 (2020). <https://doi.org/10.1039/c9ta13610j>
79. J. Wang, R. Xu, Y. Xia, S. Komarneni, Ti_2CT_x MXene: a novel p-type sensing material for visible light-enhanced room temperature methane detection. *Ceram. Int.* **47**, 34437–34442 (2021). <https://doi.org/10.1016/j.ceramint.2021.08.357>
80. C. Qiao, H. Wu, X. Xu, Z. Guan, W. Ou-Yang, Electrical conductivity enhancement and electronic applications of 2D $\text{Ti}_3\text{C}_2\text{T}_x$ MXene materials. *Adv. Mater. Interfaces* **8**, 2100903 (2021). <https://doi.org/10.1002/admi.202100903>
81. L. Chen, X. Shi, N. Yu, X. Zhang, X. Du et al., Measurement and analysis of thermal conductivity of $\text{Ti}_3\text{C}_2\text{T}_x$ MXene films. *Materials* **11**, 1701 (2018). <https://doi.org/10.3390/ma11091701>

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